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Probing the circuits of conscious perception with magnetophosphenes

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Abstract

Background: We aimed at characterizing, in non-invasive human brain recordings, the large-scale, coordinated activation of distant brain regions thought to occur during conscious perception. This process is termed ignition in the Global Workspace Theory, and integration in Integrated Information Theory, which are two of the major theories of consciousness.

Approach: Here, we provide evidence for this process in humans by combining a magnetically-induced phosphene perception task with electroencephalography. Functional cortical networks were identified and characterized using graph theory to quantify the impact of conscious perception on local (segregation) and distant (integration) processing.

Main results: Conscious phosphene perception activated frequency-specific networks, each associated with a specific spatial scale of information processing. Integration increased within an alpha-band functional network, while segregation occurred in the beta band.

Significance: These results bring novel evidence for the functional role of distinct brain oscillations and confirm the key role of integration processes for conscious perception in humans.

Keywords: electroencephalography, conscious perception, functional connectivity, brain stimulation

Introduction

The characterization of the physiological mechanisms that enable conscious perception is the focus of intense, multi-disciplinary research efforts. As opposed to the question of the nature of consciousness itself (referred to as the “hard problem” of consciousness (Harnad, 1998)), the identification and characterization of the physiological processes that enable the emergence and maintenance of consciousness (referred to as the “easy problem” of consciousness (Harnad, 1998)) is more readily achievable. Two theories of consciousness are currently dominant in the field, namely the Global Workspace Theory (GWT (Dehaene et al., 1998; Dehaene et al., 2006; Dehaene and Changeux, 2011)), and the Integrated Information Theory (IIT (Tononi, 2004)). While both share some key common points, such as information processing being at the core of conscious processes and that information needs to be *integrated* at a large scale to be efficiently shared and processed, IIT also posits that conscious experience involves a sufficiently “complex” level of information processing. Another recent theory, the Kolmogorov theory (KT) of consciousness (Ruffini, 2017), also establishes links between the algorithmic complexity of information processed by cortical networks and conscious processes. The idea that information processing coordinated between distant brain regions is essential has received considerable experimental support, notably from combined transcranial magnetic stimulation-electroencephalography (TMS-EEG) studies in disorders of consciousness (DOC) patients and healthy controls: during unconsciousness (e.g., deep sleep, Propofol anesthesia or coma), TMS-evoked EEG responses fail to propagate in cortico-cortical networks and only induce local activation, while complex spatiotemporal responses are evoked at the brain-scale during wakefulness (Casali et al., 2013).

One of the processes proposed to enable the large-scale cortical activation associated with conscious processes is termed *ignition* in GWT, and consists of a sudden and coordinated large-scale recruitment of distant brain regions that can make information

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3 available to the global workspace, enabling information processing (Dehaene and Changeux,
4 2011). Ignition has been identified using functional MRI (fMRI) in a variety of tasks, as
5 reviewed by Dehaene and Changeux (Dehaene and Changeux, 2011). A compelling example
6 is that, during subliminal perception of words, the activated brain network is considerably less
7 spatially extended than during conscious perception (Dehaene et al., 2001). Using EEG and
8 magnetoencephalography (MEG), it has also been shown that a large-scale activation in the
9 beta band within the fronto-parieto-temporal network is involved in the report of target
10 stimuli (Gross et al., 2004). Invasive intracranial recordings have also been performed in
11 humans using deep electrodes during exposure to masked/unmasked words, which revealed
12 an increase in gamma power in distant sites in association with a beta synchrony increase. In a
13 recent experimental study, van Vugt et al. provided compelling evidence for the ignition
14 process in monkeys, using intracranial electrodes during a phosphene perception task (van
15 Vugt et al., 2018). Phosphenes are visual perceptions in the absence of light, and can triggered
16 by electric stimulation (electro-phosphenes (Lovsund et al., 1980a)) or magnetic stimulation
17 (magneto-phosphenes (Lovsund et al., 1980b)). In this study, van Vugt et al. performed
18 intracranial stimulation of the visual cortex in monkeys at different current intensities (sub-
19 threshold vs. supra-threshold) and linked visual saccades with phosphene perception.
20 Consistent with predictions from GWT or IIT, large-scale brain activation was observed at the
21 onset of phosphene perception.
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47 In the present study, we aimed at inducing magnetophosphene percepts to characterize
48 non-invasively the associated ignition process in humans. Our study involved twenty human
49 subjects exposed to a 50 Hz magnetic field (MF) at 11 different flux density conditions given
50 in a random order (5 mT steps ranging from 0 -sham- to 50 mT, each repeated 5 times for a
51 total of 55 epochs per subject), while dense-EEG (64 channels) was recorded. Each epoch of
52 exposure lasted 5 seconds, which was chosen to keep reasonable the duration of the
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3 experiment. MF exposure was delivered through a whole-brain exposure system designed and
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5 manufactured in-house (Fig. 1A), which exposed the whole brain and eyeballs to a
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7 homogeneous level of MF. Large-scale functional connectivity was estimated from dense-
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9 EEG measurements using source connectivity analysis (Hassan and Wendling, 2018), and
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11 graph theory metrics were used to quantify local and global/distant processing, enabling the
12
13 identification of nodes in a cortical network. The study design is summarized in Fig. 1. Our
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15 hypothesis was that, during suprathreshold (conscious) magnetophosphene perception, a
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17 drastic increase in global/distant processing characteristic of ignition occurs, which should be
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19 detectable through an increase in network integration quantified by graph theory based
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21 metrics.
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29 **Materials and Methods**

30 *Experimental protocol*

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33 This study was approved by the Health Sciences Research Ethics Board of Western
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35 University (London, ON, Canada) under the reference HSREB#18882. All experiments were
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37 performed in accordance with the relevant guidelines and regulations. Informed consent was
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39 obtained for the N=20 healthy volunteers who were recruited (age: 23.4 +/- 1.4, 10 males and
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41 10 females). Exclusion criteria ensure that study participants had no cardiovascular,
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43 neurological or visual system disorder. They were equipped with a 64 MRI-compatible EEG
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45 cap (Maglink, Compumedics-Neuroscan, US). Subjects were asked to sit in the chair placed
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47 below the MF exposure device and the coils were lowered so subjects had their head
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49 centered in the device for the duration of the experiment. EEG was continuously recorded,
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51 and subjects were asked to remain eyes closed for the duration of the experiment. An
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53 adaptation time to the darkness of the room of 5 minutes was present at the beginning of the
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55 exposure sequence. The 55 MF exposure conditions were then randomly delivered through a
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3 custom-made LabView (National Instruments, USA) program, had a duration of 5 seconds
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5 each, and were separated by 5 seconds. Each time that the participant began to perceive
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7 magnetophosphenes, he/she had to press as fast as possible on a button directly synchronized
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9 with the EEG acquisition system.
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14 *MF exposure device and physical principles*

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17 The MF exposure device was used to deliver whole-brain exposure and consisted of
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19 “Helmholtz-like” coils designed and manufactured in-house (for full details, please refer to
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21 (Keenlside et al., 2013)). Let us mention that Helmholtz coils are a standard setup in physics
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23 dating back to the end of the 19th century. The mean diameter of each coils was 50 cm and
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25 their width 7.3 cm, and coils were separated by 20 cm. Water cooling (0.8 L/min) was used
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27 through the squared hollow wire in order to prevent coil heating. MRI gradient amplifiers
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29 (MTS corporation, USA) were used to power each coil (up to 200 A_{rms} capability). The
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31 experimental setup was Medical Grade approved by the Canadian Standard Association
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33 (CSA). The MRI gradient amplifiers driving a 50 Hz current through the coils, which per
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35 Maxwell-Ampere’s law generated a homogeneous 50 Hz MF at the level of the head and
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37 eyes, which resulted in an induced electric field at the same frequency in these exposed
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39 biological structures. Therefore, the MF exposure non-invasively generated induced fields and
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41 current in the brain and retinal tissues at 50 Hz. Furthermore, let us note that the homogeneity
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43 zone of the field included the entire brain (Keenlside et al., 2013).
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51 *EEG acquisition and processing pipeline*

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53 64-channel EEG was acquired at a sampling frequency of 10 kHz and down-sampled
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55 to 1 kHz. EEG data was imported into Matlab, and band-pass filtered between (3-35 Hz) to
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57 remove artefacts present in the signal due to the MF exposure at 50 Hz. Importantly, the entire
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3 experiment was also performed using a phantom (watermelon) with the EEG cap that was
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5 setup in the exact same manner than with participants, to validate the pre-processing step.
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7 More specifically, the same EEG cap than the one used in the experimental human study was
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9 put on a watermelon, and all electrodes were filled with electrolyte to decrease impedance, as
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11 done in actual participants. Two thin wires were inserted in the watermelon, and connected to
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13 a current generator to apply a constant current at 10 Hz (alpha frequency), with an intensity
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15 calibrated to generate a detectable current at the EEG electrode level of approx. 50
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17 microvolts, i.e. an amplitude comparable to an actual EEG. This provided us with a “ground
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19 truth” EEG to test if the processing pipeline removing MF exposure artefacts was altering the
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21 actual EEG. Then, the watermelon was setup in the MF exposure device, and the entire MF
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23 exposure protocol was ran. The acquired EEG was then filtered and we verified that the
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25 artefact-free reconstructed EEG was identical to the ground truth EEG, confirming that our
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27 processing pipeline was not altering the EEG and not biasing further connectivity analyses.
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33 For each EEG recording, the 55 EEG epochs (11 MF exposure conditions, each
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35 repeated 5 times) were extracted and imported in the Brainstorm Matlab package (Tadel et al.,
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37 2011). The entire duration (5 seconds) of each epoch was extracted, and a window function
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39 was applied (Hamming window) to avoid edge effects.
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42 Nasion-inion and preauricular anatomical measurements were made to locate each
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44 individual’s vertex site. Electrode impedances were kept below 10 kOhm. EEG signals are
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46 frequently contaminated by several artifacts sources, which were addressed using the same
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48 preprocessing steps as described in several previous studies dealing with EEG resting-state
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50 data (Kabbara et al., 2017; Kabbara et al., 2018). Briefly, bad channels (signals that are either
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52 completely flat or contaminated by movement artifacts) were identified by visual inspection,
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54 complemented by the power spectral density. These bad channels were then recuperated using
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56 an interpolation procedure implemented in Brainstorm (Tadel et al., 2011), using neighboring
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3 electrodes within a 5 cm radius. Epochs with voltage fluctuations $> +80 \mu\text{V}$ and $< -80 \mu\text{V}$
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5 were removed.
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10 *Magnetophosphene reports*

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12 Subjects were instructed to report magnetophosphene perception by using a button
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14 press as soon as they could when the perception began. Subjects were instructed to press only
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16 once, however a custom Matlab code was developed to detect and remove possible “double
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18 presses” which could accidentally occur.
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26 *Brain networks reconstruction*

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28 Functional brain networks were reconstructed using the EEG source-space
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30 connectivity method (Hassan et al., 2014; Hassan and Wendling, 2018), which includes two
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32 main steps: 1) reconstruct dynamics of the cortical sources by solving the inverse problem,
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34 and 2) measure the statistical couplings (functional connectivity) between the regional time
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36 series. The EEG source connectivity method links the recorded scalp EEG signals with the
37
38 functional relationships between anatomical brain regions (e.g., networks), through the EEG
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40 inverse problem that provides the localization of the cortical sources originating these EEG
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42 signals. Several methods exist for both of these two steps (EEG inverse problem and
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44 functional connectivity measures). Here, we used the weighted minimum norm estimate
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46 (wMNE) algorithm as an inverse solution. The reconstructed regional time series were filtered
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48 in different frequency bands (theta, 4-7 Hz; alpha, 8-12 Hz; beta; 13-30 Hz). For each
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50 frequency band, functional connectivity was computed between the regional time series using
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52 the phase locking value (PLV) measure (Lachaux et al., 1999). The wMNE/PLV combination
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3 was chosen according to recent model-based and data-driven comparative studies of different
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5 inverse/connectivity combinations (Hassan et al., 2017).
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10 EEGs and structural MRI template (ICBM152) were co-registered through the
11 identification of anatomical markers using Brainstorm (Tadel et al., 2011). A Desikan-
12 Killiany atlas-based segmentation approach was used, consisting in 68 cortical regions
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14 (Desikan et al., 2006). The OpenMEEG (Gramfort et al., 2010) software was used to compute
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16 the three-layer (scalp, skull and brain) model. The functional connectivity between the 68
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18 regional time series was computed using the PLV, using EEGNET (Hassan et al., 2015; Tadel
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20 et al., 2011), for each condition, in the different frequency bands. This resulted for each
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22 subject, in each of the three frequency bands, in 55 68x68 connectivity matrices (one per MF
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24 condition). Finally, we only kept the strongest 10% of connections (proportional threshold).
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33 *Characterization of functional networks*

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35 Our main objective was to explore two important properties related to information
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37 processing in the human brain network:
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40 - **Network segregation**, which reflects local information processing. For this reason,
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42 the clustering coefficient 'Cc' was computed, considered as a direct measure of network
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44 segregation (Bullmore and Sporns, 2009). In brief, Cc represents how close a node's
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46 neighbors tend to cluster together (Watts and Strogatz, 1998). This coefficient is the
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48 proportion of connections among a node's neighbors, divided by the number of connections
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50 that could possibly exist between them, which is 0 if no connections exist and 1 if all
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52 neighbors are connected.
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56 - **Network integration**, which reflects global information processing. The
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58 participation coefficient was computed to measure the diversity of node inter-modular
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3 connections (Guimera and Amaral, 2005). The participation coefficient (P_c) of a node is close
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5 to 1 if its links are uniformly distributed among all the modules and 0 if all of its links are
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7 within its own module. Nodes with high participation coefficients interconnect multiple
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9 modules together, and hence can be seen as connectivity hubs. At the group level, this
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11 resulted in a C_c and P_c matrix for each of the 68 ROIs in each of the 55 MF conditions, for
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13 each frequency band.
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17 We have chosen to focus on those two graph metrics, clustering and participation for the
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19 reason that, many different metrics exist, and one cannot simply apply all of them to identify
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21 one that is significant. Therefore, we have rather chosen to use specific metrics that are
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23 directly linked with the hypothesis being tested. Since two of the main theories of
24
25 consciousness, namely the Global Workspace Theory (GWT) and the Integrated Information
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27 Theory (IIT), explicitly emphasize the role of integration/distant processing, we have chosen
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29 to use the participation coefficient that quantifies the connectivity between distant
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31 regions/modules. Furthermore, the concept of differentiation is linked with the clustering
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33 coefficient, and is another key concept in terms of the neuronal processes associated with
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35 consciousness (Koch et al., 2016). Consequently, we have focused in this study exclusively
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37 on the parameters of clustering and participation that are directly linked with the question
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39 addressed and its conceptual framework, i.e. the maintenance of conscious processes through
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41 long-distance communication between brain regions.
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46 47 *Statistical analysis*

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49 First, the Pearson correlation between the C_c/P_c matrix and the reported perception
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51 curve (probability of perception between 0 and 1, computed for each condition as the number
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53 of button presses divided by the number of repetitions, i.e. 5) was computed using Matlab and
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55 the False-Detection Rate (FDR) method was used to account for multiple comparisons. In this
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57 paper, we used the Benjamini and Hochberg (B-H) procedure, see (Thissen et al., 2002)
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3 which consists in adapting the new threshold to each resultant p-value instead of using the
4 same threshold as suggested in Bonferroni correction. The graph theoretical metrics were
5 computed using the Brain Connectivity Toolbox (Rubinov and Sporns, 2010). Second, the
6 linear trend associated with increasing MF flux density was assessed using the Jonckheere-
7 Terpstra test (implemented in Matlab, The Mathworks, USA) with correction of the
8 significance threshold using the FDR. The correlation with the (non-linear) perception curve
9 was assessed using a linear correlation (Matlab, The Mathworks, USA) corrected using FDR.
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21 *Quantification of the ignition process*

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23 To quantify the ignition process, the functional connectivity matrices were averaged
24 over subjects at each flux density value (averaged also over five trials). The degree of each
25 brain region, i.e. its number of functional connections, was then computed (after keeping the
26 highest 50% of connections, keeping in mind that this threshold was used to estimate the
27 connections with the highest degree, and not the strongest connections, for which a
28 proportional threshold of 10% was used as aforementioned). The ignition process is therefore
29 considered as the increased number of functional long-range connections when the probability
30 of perception increases.
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45 *Software*

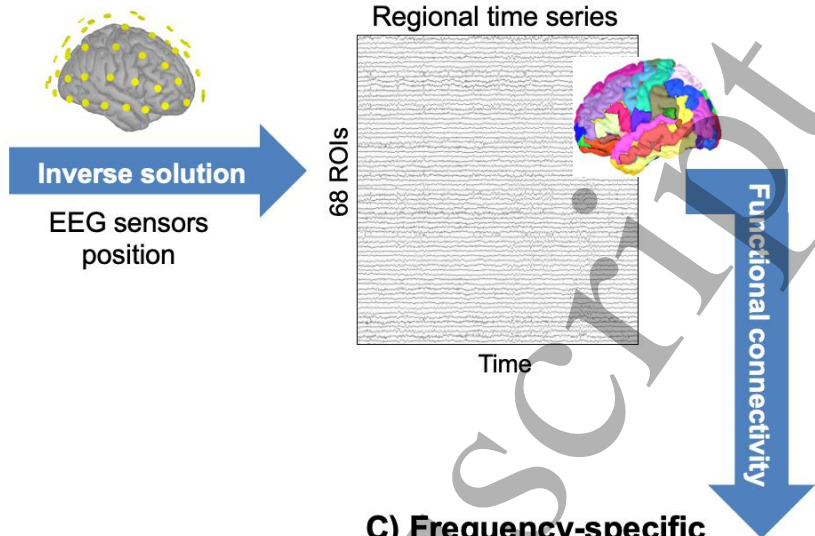
46 The functional connectivity, network measures and network visualization were
47 performed using BCT (Rubinov and Sporns, 2010), EEGNET (Hassan et al., 2015) and
48 BrainNet viewer (Xia et al., 2013), respectively.
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54 The study design is summarized in Figure 1 below.
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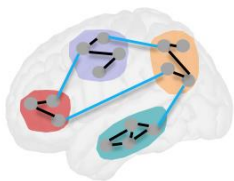
**A) Data recordings:
MF exposure + dense EEG**



B) Reconstruction of brain sources



**D) Metrics of network
integration and segregation**



**C) Frequency-specific
functional brain networks**

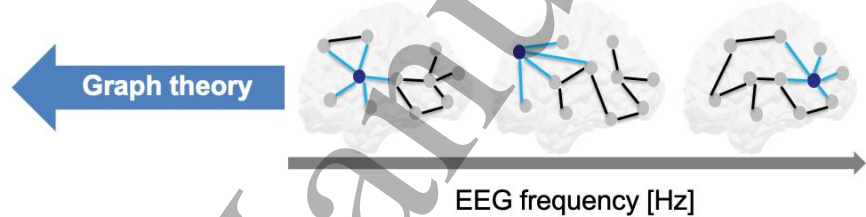


Fig. 1. Study design and data analysis pipeline. **A)** MF exposure setup (water-cooled Helmholtz coils, in-house design and engineering, see Methods for details) used to induce magnetophosphene perception. Subjects could report magnetophosphene perception using a button press. Dense-EEG (64 channels, MRI compatible cap) was recorded throughout the entire experiment. Informed consent of the study participant was obtained for the publication of this picture in an online open-access publication. **B)** Source activity was reconstructed for the 68 regions of the Desikan-Killiany atlas. **C)** Frequency-specific functional networks were computed for the theta, alpha and beta frequency bands. **D)** Metrics from graph theory were used to quantify segregation and integration (local and global processing, using clustering and participation coefficients, respectively).

Results

As expected, participants did not perceive phosphenes in the sham condition (0 mT), as seen in Fig. 2, and the perception of magnetophosphenes, as assessed by perception button-press self-reports, began with a 0.28 probability of perception at a threshold value of 20 mT when the entire head was stimulated by the homogeneous 50 Hz sinusoidal signal. It is worth noting that, at the maximal MF flux density value used (50 mT), the probability of magnetophosphene perception was close to 1 (0.96). Phosphene perception was reported by all subjects as colorless, stroboscopic dots/lines. The resulting magnetophosphene perception curve as a function of the MF flux density results in a sigmoid-like function, as can be seen in Fig. 2 (lower panel), similarly to the curve obtained in monkeys with increasing intracranial stimulation current values (van Vugt et al., 2018). The comparison between these two curves is direct: intracranial current injection results in an electric field that depolarizes neighboring neuronal elements, while MF exposure also induces an electric field in brain tissue per Maxwell-Ampere's law of magnetic induction. One difference is that, in the present study, retinal cells instead of visual cortex cells are modulated by the induced electric field. As detailed in the Methods section, each functional network reconstructed in each of the 55 conditions featured 68 ROIs, and the participation and clustering coefficients quantifying *integration* (global) and *segregation* (local) processing respectively, were computed for each frequency band (theta, 4-7 Hz; alpha, 8-12 Hz; beta, 13-30 Hz). Gamma-band networks were not estimated due to the need of filtering the EEG from 50 Hz stimulation contamination, and to avoid possible biases. In the following, all *p*-values were corrected for multiple comparisons using the False Detection Rate (FDR) method.

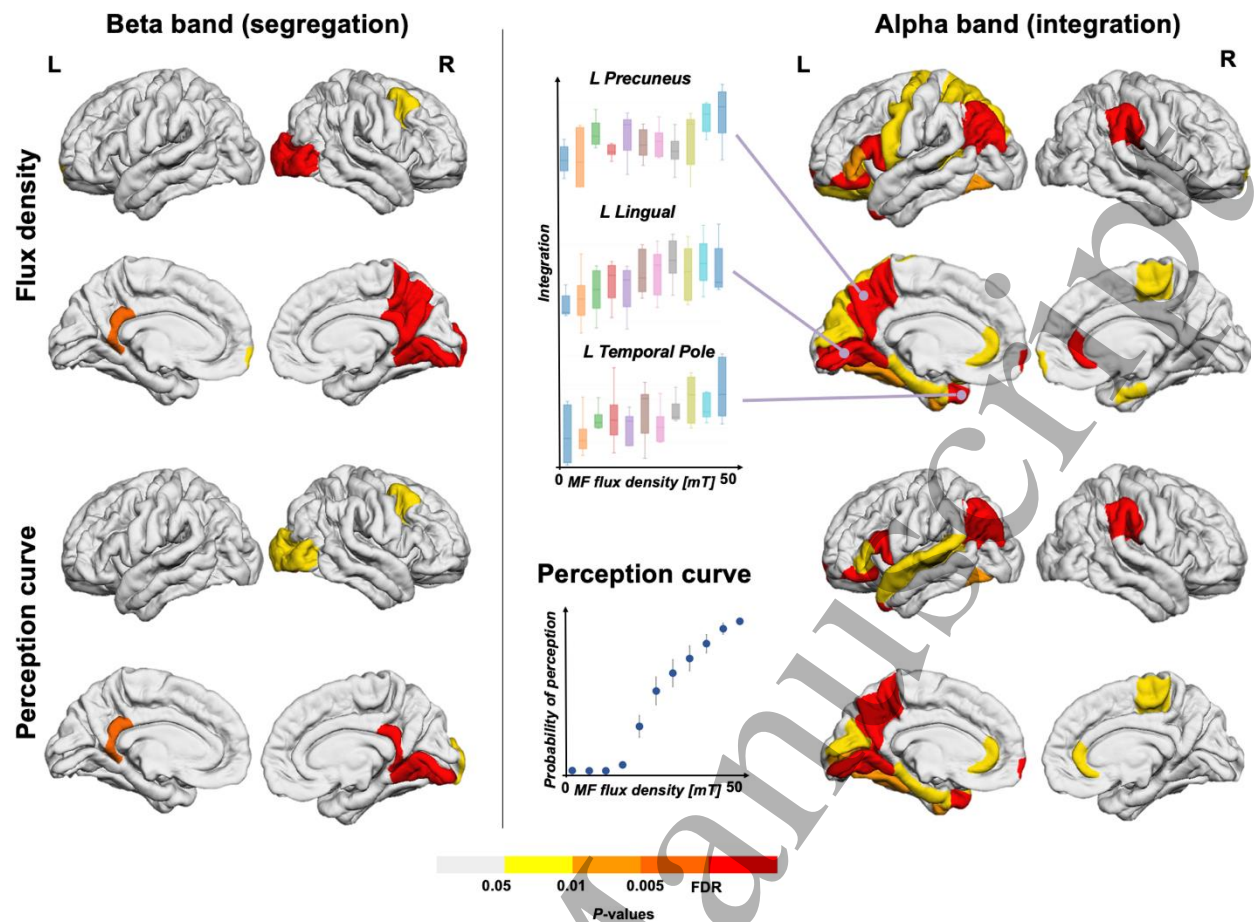


Fig. 2. Left panel. Segregation results in the beta-band functional network (linear trend, flux density sub-panel; correlated with perception reports, perception curve sub-panel). Results are presented for each hemisphere. **Right panel.** Integration results in the alpha-band functional network (linear trend, flux density sub-panel; correlated with perception reports, perception curve sub-panel). Results are presented for each hemisphere. The increase in integration with flux density is shown for three regions of interest (left precuneus, left lingual and left temporal pole), along with the perception probability curve for magnetospherene from subjective reports (N=20 subjects).

First, brain structures for which integration (quantified by the participation coefficient (Guimera and Nunes Amaral, 2005)) was correlated with the MF flux density were almost exclusively within the alpha band (see Fig. 2, right panel). More specifically, there were

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3 structures involved both in “subliminal” (i.e., 50 Hz MF exposure below the perception
4 threshold) and suprathreshold magnetophosphene perception. These regions involved DMN
5 (Default Mode Network) structures such as the right rostral anterior cingulate ($p=0.0012$) and
6 left parahippocampal gyrus ($p=0.0116$); a structure from the VIS (visual) network (left
7 fusiform, $p=0.0089$); and a DAN (Default Attention Network) structure (left pars triangularis,
8 $p=0.007$). The left pericalcarine cortex ($p=0.0052$, visual cortex area), right entorhinal
9 ($p=0.0085$), right frontal pole ($p=0.0085$), and right paracentral ($p=0.0092$) were also involved.

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19 Regions correlating specifically with the perception curve involved a DMN region (left
20 precuneus, $p=0.001$), two regions from the DAN (left pars orbitalis and left pars opercularis,
21 $p<0.001$), and a region from the SAN (Salience Attention Network), namely the right
22 supramarginal gyrus ($p<0.001$). Interestingly, the right supramarginal gyrus has been
23 previously identified as involved in phosphene perception in humans using intracranial
24 stimulation (Beauchamp et al., 2012). The left temporal pole, $p < 0.001$, the left frontal pole,
25 $p=0.0026$ and left inferior parietal, $p<0.001$ were also involved.

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Second, magnetophosphene perception was associated with an increase in segregation
(local processing) almost exclusively in a beta functional network, as illustrated in Fig. 2 (left
panel). More specifically, the network segregation increased (both for “subliminal” and
conscious perception) in the right lingual cortex ($p<0.001$, VIS), within DMN regions (right
precuneus, $p=0.0018$; and left/right isthmus cingulate, $p=0.0019$ and $p<0.001$ respectively)
and a DAN region (right caudal middle frontal gyrus, $p=0.0031$). In the case of conscious
(suprathreshold) perception, only the right lingual cortex and right isthmus cingulate ($p <$
 0.001) specifically showed significant correlation with the perception curve in terms of beta
network segregation.

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3 Notably, while magnetophosphene perception was mainly restricted to effects within
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5 alpha- and beta-band functional networks, a limited number of brain structures displayed
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7 increased integration within the theta (left pars triangularis, $p < 0.001$; right middle temporal,
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9 $p = 0.001$) and beta (left precuneus, $p < 0.001$) bands. Furthermore, regarding network
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11 segregation, an effect was also identified in a single region (right superior frontal gyrus,
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13 $p < 0.001$) of the alpha functional network. It should also be noted that there was an asymmetry
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15 between hemispheres in terms of regions involved. This is consistent, for example, with the
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17 known hemispheric specialization of occipito-temporal pathways depending on the spatial
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19 resolution of visual stimuli (Kauffmann et al., 2014).
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25 In addition, we also compared how integration and segregation varied when the
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27 stimulus (MF) was kept constant, but conscious awareness was different (report versus no
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29 report). This was done both at the individual- and group-levels. For the individual level, we
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31 used for each subject the condition that was associated with a probability of perception as
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33 close as possible to 50% (either 2 or 3 perceptions out of 5 repetitions). For the group level,
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35 the 25 mT condition was retained since it was associated with a mean perception probability
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37 of 54%. In both analyses, the participation and clustering coefficient for “seen” epochs versus
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39 “unseen” epochs were compared for each ROI, including a FDR correction for multiple
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41 comparisons. Using individual perception thresholds, only one region had increased
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43 integration in the “seen” condition (right orbitofrontal cortex, $p = 0.0001$), and in the theta
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45 band only. No ROI had significantly different clustering coefficients. When using the group
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47 perception threshold of 25 mT, no ROI had significantly integration in any frequency band,
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49 while two ROIs had a significantly different clustering coefficient in “seen” versus “unseen”
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51 epochs: right superior parietal cortex ($p < 0.0004$) and the left pars orbitalis ($p = 0.0012$).
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57 Finally, we deciphered the ignition process during the conscious perception of
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59 magnetophosphenes (Fig. 3) during increased MF flux density, corresponding to a higher
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level of retinal stimulation. In this example, the number of functional connections of the left precuneus (one of the regions achieving the highest significance regarding integration in the alpha band) to distant regions, including frontal regions, increases with the probability of perception.

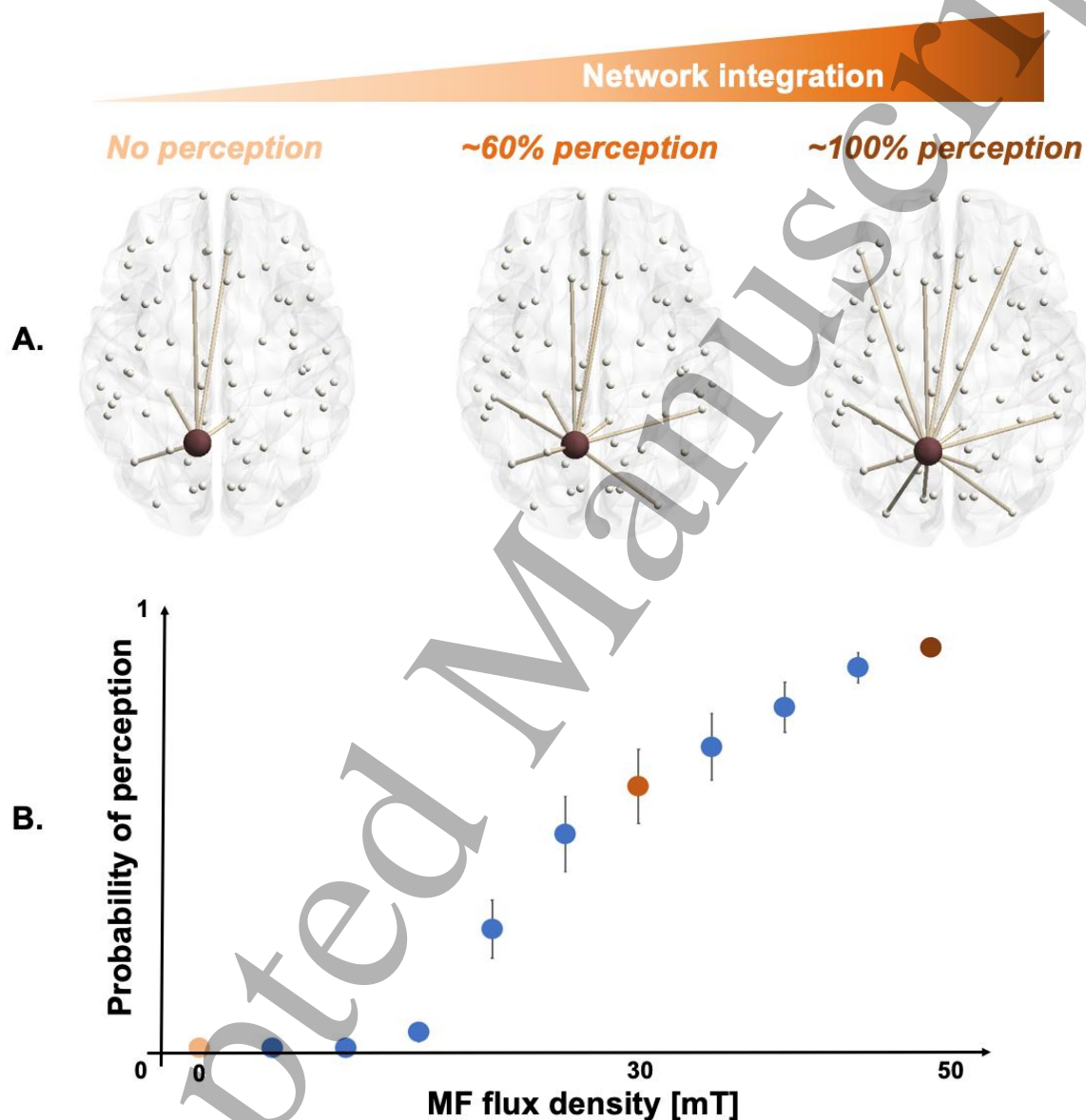


Fig. 3. **A.** Illustration of the ignition process occurring with the increase of long-range connections (in this example, from the left precuneus) associated with the increase in probability of magnetophosphene perception at 0 mT (left), 30 mT (middle) and 50 mT (right). **B.** Probability of magnetophosphene perception curve from the N=20 subjects

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3 between 0 and 50 mT, with the 0 (light orange), 30 (orange) and 50 mT (burgundy) points
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14 This drastic increase in the functional connections between the left precuneus (a
15 critical region from the DMN) and distant regions emphasize the central role of long-range
16 connectivity for the emergence of conscious perception. Interestingly, long-range functional
17 connections at baseline (without perception) remain present when the perception probability
18 increases, while novel long-range connections gradually appear. Here, we have focused this
19 figure on the left precuneus, since this region was one of the most significantly correlated
20 with conscious perception in terms of integration within the alpha band. Furthermore, the
21 precuneus has been shown to be central in several studies of patients suffering from disorders
22 of consciousness. For example, it has been shown that an hypo-metabolism within the
23 precuneus was observed in Unresponsive Wakefulness Syndrome (Annen et al., 2016), and
24 that an increase in metabolism was observed within this region after emergence from
25 Minimally Conscious States (Laureys et al., 2006).
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44 **Discussion**

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46 Magnetophosphene perception increases as a function of the increasing level of
47 magnetic stimulation, which results from the induced electric fields modulating retinal neuron
48 signaling (Attwell, 2003). The increase in magnetophosphene perception probability induced
49 in healthy human volunteers results in an increase of information integration at the brain-scale
50 in the alpha band. Conscious perception was tracked using participant subjective reports and
51 increased with gradually increasing stimulus strength. The frequency-dependent increase of
52 information integration was observed mostly in visual- and DMN-related regions, and also in
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3 a few frontal regions. We also identified an increase in the number of functional connections
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5 mostly in the alpha band between one of the most critical nodes of the identified cortical
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7 network, namely the left precuneus, and distant regions, when the probability of perception
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9 increased. To our knowledge, this is the first use of EEG source-space networks to
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11 characterize the increase of integration information as a consequence of conscious visual
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13 perception. These results are in line with the recent study by van Vugt et al. (van Vugt et al.,
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15 2018) who identified the ignition process in monkeys, also using a phosphene perception
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17 paradigm (with stimulation delivered intracranially, as opposed to non-invasively in the
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19 present study). Taken together, these results provide further support for the ignition process
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21 that was conceptualized in GWT, and also for the integration concept at the core of IIT. While
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23 our results did not provide a definite illustration of the ignition process in humans during
24
25 conscious perception, our results obtained through the EEG source connectivity technique
26
27 hint at this process. In order to obtain a more definite answer, possibilities include performing
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29 a larger number of repetitions per condition at the individual perception threshold, and/or
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31 increasing the sample size. Taken together, our results suggest an increase of integration
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33 during conscious perception in a limited number of brain regions, in low-frequency rhythms
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35 (theta, alpha). This is in line with our recent proposal that low-frequency rhythms enable the
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37 “locking” between distant brain regions, while higher-frequency rhythms (generated more
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39 locally) are involved in information transfer itself (Modolo et al., 2020).

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42 Interestingly, changes in integration (quantified using the participation coefficient) were
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44 mostly within low-frequency bands (theta, alpha), while changes in segregation (quantified
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46 using the clustering coefficient) were mostly within a higher-frequency band (beta). This
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48 supports the idea that low-frequency oscillations such as theta and alpha are involved
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50 establishing transient communication between distant brain regions and shaping the global
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52 architecture of functional networks (e.g., Gating by Inhibition, see (Bonfond et al., 2017),
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3 and review in (Modolo et al., 2020)), while high-frequency rhythms are rather involved in the
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5 processing of information, an example being communication through coherence (CTC, (Fries,
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7 2005)). Consequently, our results pertaining to conscious perception support this general view
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9 about the general function of neuronal oscillations in terms of establishing and activating
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11 transient functional networks in general, and in conscious process in particular. Another
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13 originality of this study is that we characterized the functional networks involved in the
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15 biological effect occurring at the lowest known level of *in situ* electric field, which may
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17 provide further arguments for the use of magnetophosphene perception to define international
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19 safety electromagnetic exposure guidelines (IEEE, 2010; International Commission on Non-
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21 Ionizing Radiation, 2010).
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26 One limitation of our approach is the use of EEG source reconstruction, which is not
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28 free of biases. Numerous different methods have been indeed proposed to reconstruct source-
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30 level activity from EEG (scalp) signals and differ by their hypotheses regarding the spatial
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32 extent or number of sources, for example. Therefore, it is not surprising that those algorithms
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34 can result in slightly different estimations of the underlying cortical sources [Mahjoory et al.,
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36 2017]. It has also been shown that connectivity measures can provide indeed quite different
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38 estimates [Mahjoory et al., 2017], which has to be kept in mind when selecting measures of
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40 functional connectivity. In this paper, we have used the wMNE source reconstruction method,
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42 that was shown to provide when used in combination with PLV the best estimation of ground
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44 truth cortical sources [Hassan et al., 2013]. Finally, one should be cautious about comparing
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46 those EEG-based results with fMRI studies, since the relationship between the BOLD signal
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48 and EEG signals in specific frequency bands is highly complex, as discussed in [Scheeringa et
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50 al., 2016].
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55 Another limitation in our study is that the whole brain was exposed to the delivered MF,
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57 which leaves open the possibility that some identified brain regions were not necessarily
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3 associated with phosphene perception, but rather with neuromodulation from the MF. Our
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5 whole head exposure protocol was chosen since it is the most effective to generate
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7 phosphenes perception non-invasively, which was the most important required feature at this
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9 initial stage of evaluating if brain networks would react to this perception. The MF exposure
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11 device was very different from a TMS (transcranial magnetic stimulation) device in the
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13 following respects: 1) the resulting MF flux density was much lower (0.05 T here versus > 1
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15 T for TMS devices); 2) the level of dB/dt (proportional to the current induced in brain tissue)
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17 was much lower (approx. 15 T/s here versus > 10,000 T/s for TMS devices); 3) TMS targets a
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19 relatively narrow brain region typically at spiking suprathreshold levels, while the present
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21 exposure device provides whole-brain exposure at subthreshold levels (no neuronal firing
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23 outside of the retina can be directly induced by the MF used in this study even at the highest
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25 flux density -50 mT-, as detailed below); 4) TMS uses very short pulses (typically 100 μ s)
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27 while the present MF exposure can deliver MF during minutes continuously. Next
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29 developments will use a more focal stimulus targeting the eyeball. Let us mention that the MF
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31 stimulation device used in this study was originally designed and built to study non-invasive
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33 neuromodulation thresholds inducing systematic acute responses in humans for the purpose of
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35 documenting international guidelines and standards regarding human electromagnetic field
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37 exposure. The main advantage of this non-invasive stimulation modality applied to the visual
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39 system is that the stimulus can be delivered even in an apparently unconscious patient with
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41 the eyes closed, to whom it would not be possible to present stimuli on a screen. For these
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43 reasons, and because brain functions associated with conscious visual awareness are well
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45 studied and well understood, better than for auditory awareness (acknowledged for example
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47 by (Snyder et al., 2012)), we chose to study how the circuits of visual perception would
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49 respond to such stimulation of visual pathways.
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3 That being said, one critical point is that the levels of MF flux density in this study,
4 and delivered during such short durations (5 seconds), are known to *activate the retina only*,
5 since the perception of magnetophosphenes is the biological effect occurring at the lowest
6 known MF flux density: it is precisely for this reason that the international guidelines
7 protecting the general public and workers from the adverse effects from electromagnetic
8 fields exposure are based, for extremely low-frequency fields (< 300 Hz), on the perception of
9 magnetophosphenes (IEEE, 2010; International Commission on Non-Ionizing Radiation,
10 2010). Therefore, from the existing literature, direct acute effects of the MF delivered here on
11 another system than the retina, is, according to the current existing literature, extremely
12 unlikely. This supports further that the observed changes in functional connectivity are indeed
13 associated with the perception of magnetophosphenes. Another limitation is that, since we
14 used a 50 Hz stimulus, we were not able to investigate gamma-band functional networks. A
15 50 Hz frequency was selected because it is reported to be effective in triggering phosphene
16 perception (phosphene perception decreases as the stimulus frequency increases), although
17 the related contamination of EEG signals involves filtering and thereby prevents investigation
18 of gamma-related processes.
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40 In addition to a contribution in terms of the fundamental mechanisms of
41 consciousness, we also suggest that our experimental paradigm could form the basis of a
42 novel protocol to probe conscious processes in humans. While a rather cumbersome
43 experimental setup was used in this study, it would be possible to simplify it by using scalp
44 (surface) electrodes placed on the temples and with an adapted level of delivered electrical
45 current. One could also argue that a more conventional visual stimulation at different
46 intensities could be used, avoiding the complications linked with the use of brain stimulation.
47 However, we have in mind the potential to use integration as a possible measure of residual
48 conscious processes, for example in minimally conscious patients. In those patients, blindness
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3 can occur due to cornea dryness, preventing the use of classical stimulation protocols. Since
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5 magnetic stimulation bypasses the cornea and directly impacts the retina, such issue would
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7 not occur with our method, opening the possibility to develop neuromodulation-based
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9 protocols of consciousness evaluation while requiring considerable less power than existing
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11 TMS protocols. Furthermore, this work identifies a key brain region in the conscious
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13 perception of a visual stimulus, namely the precuneus, a brain region that has been shown to
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15 be key for the maintenance of consciousness (Cavanna and Trimble, 2006). Hence, our results
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17 bring support for a role of the precuneus not only in “basal” consciousness, but also in the
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19 perception of external stimuli (conscious perception).
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24 Another more fundamental implication of these results is that the spatial extent of
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26 functional network dynamics and frequency processing is frequency dependent: during
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28 magnetophosphene perception, distant information processing increases mostly within the
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30 alpha band, while local information processing increases mostly within the beta band. This
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32 result is consistent with other studies pointing to the role of low-frequency oscillations for
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34 distant communication between brain regions, while higher frequency rhythms would rather
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36 contribute to stimulus encoding itself (Lisman and Jensen, 2013). Therefore, our results bring
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38 further support to the framework conceptualizing information flow and processing between
39
40 brain structures as an interplay between slow and fast oscillations, each associated with a
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42 “range” for information processing and a specific functional role.
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47 **Conflicts of interest:** The authors have no competing financial or non-financial interests to
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49 declare.
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51 52 **References and Notes**

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9 **availability:** EEG data and analysis pipeline details are available upon reasonable request.

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20 "The authors have confirmed that any identifiable participants in this study have given their consent
21 for publication".
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