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1 **Alternative left ventricular pacing approaches for an optimal cardiac resynchronization**
2 **therapy**

3

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19

1 **ABSTRACT**

2

3 Cardiac resynchronization therapy (CRT) improves mortality, morbidity and quality of life in
4 selected heart failure patients with severe left ventricular ejection fraction impairment.
5 However, between 20% and 40% of device recipients do not benefit clinically from CRT.
6 Indeed, some anatomical and technical difficulties are related to the coronary venous
7 implantation site via the coronary sinus (CS). Additionally, electrical constraints have been
8 described and CS does not always correspond to the optimal LV lead position. In the last
9 decade, engineers and physicians work together to overcome the challenging LV lead
10 implantation and various bi-ventricular pacing alternatives have been developed to improve
11 CRT response. In this review, we discuss the evolution from the CS pacing to wireless LV
12 stimulation and His bundle pacing.

13

14 **KEY WORDS:** Cardiac resynchronization therapy, non-responder, optimal left ventricular
15 lead location, endocardial stimulation, leadless stimulation

1 INTRODUCTION

2

3 Cardiac resynchronization therapy (CRT) improves mortality, morbidity and quality of
4 life in selected heart failure (HF) patients with severe left ventricular ejection fraction (LVEF)
5 impairment (1-7). Left ventricular (LV) pacing is conventionally achieved with an epicardial
6 LV lead, placed into one of the branches of the CS, mainly lateral or postero-lateral in
7 location. However, between 20% and 40% of device recipients do not benefit clinically from
8 CRT (7). In addition, some patients eligible do not receive CRT due to anatomical and
9 technical difficulties, such as an unsuitable CS anatomy, chronic occlusion of venous access,
10 phrenic nerve stimulation or high pacing threshold in areas of extensive myocardial scar (8-9).

11 To overcome these challenges, bi-ventricular pacing alternatives have been described,
12 such as surgical epicardial leads or transeptal LV endocardial leads (10-12). However, these
13 strategies expose the patient to high surgical risks for the epicardial approach or ischemic
14 stroke for endocardial approach (13). Furthermore, the lead remains the Achilles heel of these
15 strategies. Nevertheless, LV endocardial (LVendo) pacing has shown promising results and
16 may allow a higher number of site implantation locations compared to conventional CRT.
17 These encouraging effects are counterbalanced by the relative complexity of the lead
18 implantation and the risk of stroke. Currently, LVendo leadless stimulation has been
19 developed and demonstrated clinical feasibility and benefits in patients with failed CRT
20 implantation or non-response to conventional CRT (14-15).

21 In current practice, placing the LV lead via the CS is the dominant strategy with
22 sometimes anatomical limitations and thus conventional approach may not be sufficient. From
23 the CS epicardial stimulation to the leadless endocardial pacing, engineers and physicians
24 have been developing alternative LV pacing approaches to improve CRT. This review aims to

1 describe these different approaches and the evolution that has been taking place from LV
2 epicardial to LVendo techniques.

3

4 **THE BENEFIT AND LIMITS OF CARDIAC RESYNCHRONIZATION THERAPY** 5 **IN PATIENTS WITH HEART FAILURE**

6

7 There are now numerous landmark trials establishing the efficacy of CRT therapy in
8 patients with HF. MUSTIC (Multisite Stimulation in Cardiomyopathies) trial was the first to
9 evaluate the benefit of CRT in severe HF patient (NYHA III). Biventricular pacing
10 significantly improved patients' exercise tolerance, quality of life and risk of hospitalization
11 (decreased by 2/3) (1). Similarly, MIRACLE (Multicenter Insync Randomized Clinical
12 Evaluation) trial assessed the benefit of CRT in 453 patients with advanced HF (NYHA
13 III/IV) (2). Indeed, CRT was associated with LV chronic reverse remodeling, improvement of
14 the quality of life and a 40% decrease of death or HF hospitalization. Similar results were
15 reported in the CARE-HF (Cardiac Resynchronization on Morbidity and Mortality in Heart
16 Failure) trial among patients with NYHA III/IV status (3). The benefit of CRT in patients
17 with mildly symptomatic HF was assessed in the REVERSE-HF, MADIT-CRT and RAFT
18 trials, including mostly patients with NYHA I/II. In this population, CRT was associated with
19 LV reverse remodeling and a reduction in HF hospitalizations of between 25% and 50% (4-6).
20 Among these studies of mild-HF CRT recipients, the RAFT trial was the only one to show a
21 positive impact on mortality with a 25% risk reduction (6). Currently, CRT is highly
22 recommended for symptomatic HF patients in sinus rhythm with severe LVEF (<35%) and
23 large left bundle branch block (>150ms) (7) but also at a lower level in patients with LBBB
24 and QRS duration between 120 to 150 ms. For patients without LBBB the class of
25 recommendation is lower. Unfortunately, not all patients respond favorably to CRT with a

1 non-responders rate between 20% and 40% (8-10). Therefore, research related to the
2 mechanism underlying response (and failure to respond) has been performed and some factors
3 specific to each patient have been associated with a lower response rate to this therapy (e.g.
4 narrower QRS, QRS morphology, underlying cardiomyopathy).

5

6 **CORONARY SINUS VEIN: A CONVENTIONAL APPROACH WITH HIGH** 7 **BENEFIT BUT ALSO WITH LIMITS**

8

9 *Coronary sinus vein provides an optimal lead location in a majority of CRT patients*

10 Early CRT Systems took advantage of the CS anatomy to place the LV lead due to the
11 straightforward accessibility from the venous side and reasonable ability to establish and
12 maintain capture in this location. In time, this has been improved upon but remains the first
13 line approach. A crucial determinant of successful CRT is the position of the LV pacing lead.
14 Initial hemodynamic studies have recommended that targeting the lateral or posterolateral
15 wall by way of an appropriate CS branch can improve clinical outcomes after CRT. Indeed,
16 CRT with lateral free wall stimulation produced improvements in LV systolic performance
17 with a significant increase of LV+dP/dt (max) (16). Similarly, the influence of the LV lead
18 position was assessed among 346 patients of the REVERSE cohort, revealing that the lateral
19 position was associated with a significantly lower risk of HF hospitalization or death from any
20 cause compared to the non-lateral placement (17). In addition, LV apical pacing has been
21 associated with poor outcomes for CRT and this placement should be avoided. Indeed, a sub
22 analysis of the MADIT-CRT trial showed that, compared to mid-ventricular or basal pacing,
23 LV apical pacing was associated with worse clinical outcomes (18). Consequently, based on
24 the hypothesis that lateral or posterolateral sites have the latest activation in a majority of
25 patients, these implant sites are commonly preferred in patients eligible for CRT (19).

1 Through the CS vein, CRT with LV-only pacing has also been described (20). Indeed,
2 Medtronic's *AdaptiveCRT* algorithm has been developed and used the patient's intrinsic
3 conduction by pre-pacing the LV to synchronize with intrinsic right ventricular (RV)
4 activation and establish fusion. Of note, when the patient's heart rate increases > 100 bpm or
5 atrio-ventricular conduction is prolonged, the pacing mode switches automatically to bi-
6 ventricular pacing. This interesting approach aims to avoid unnecessary RV pacing and has
7 been associated with reduction in death, AF and HF hospitalization (20).

8

9 However several reports describe a considerable variability in the LV activation
10 pattern and distribution of mechanical dyssynchrony in case of typical LBBB. Consequently,
11 there is inter-individual inconsistency regarding the most optimal pacing site (21).
12 Furthermore, some CRT candidates do not have a typical LBBB morphology or present
13 ischemic cardiomyopathy, and thus likely have variable and heterogeneous LV activation
14 sequences (22). As a result, the optimal LV pacing site to restore LV synchrony does not
15 always correspond to the lateral or posterolateral branch of the CS vein and conventional
16 approach sometimes fails to improve HF patients. In addition, electrical constraints, such as
17 phrenic nerve stimulation, and occluded CS anatomy or other anatomical constraints can limit
18 procedure success.

19

20 *Coronary sinus: electrical and/or mechanical constraints*

21 Discordance between the CS and the optimal position for LV stimulation has been
22 described by Derval *et al.* (23). In this study, a cohort of 35 non-ischemic patients who
23 received CRT, LV hemodynamic (dP/dTmax) response was optimized by pacing 11 LV sites.
24 None of these positions were consistently associated with the best hemodynamic
25 improvement and the distribution of the best pacing site for each individual patient was

1 uniformly spread among the tested sites. Furthermore, CS pacing was the best pacing site in
2 only 3 patients (9%) and had no or detrimental effect in 8 patients (23%). These results are
3 consistent with results previously described by Dekker *et al.* who found that the
4 hemodynamic response to biventricular pacing varied widely based on LV site (24).
5 According to these results, the best site is not a predetermined area of the LV but rather
6 specific to each patient.

7 Whether there is any benefit in targeting the area of maximal mechanical delay was
8 studied in the prospective TARGET (Targeted Left Ventricular Lead Placement to Guide
9 Cardiac Resynchronization Therapy) study (25). In a cohort of 220 patients, the impact of
10 targeting the LV lead at the most delayed viable segment defined by speckle-tracking
11 echocardiography was compared the standard clinical practice. After 6 months of CRT, there
12 was a significantly higher rate of responders in the TARGET group compared to the control
13 group (70% vs. 55% respectively) and a lower rate of death and HF hospitalization. Although
14 imaging technique improves CRT response and avoids the LV lead placement in scar areas, it
15 is time-consuming, suffers from reproducibility and may be hard to correlate with
16 fluoroscopic imaging at the time of device implantation.

17 A more practical intra-operative measurement is the delay between QRS onset on the
18 surface ECG and the LV electrograms (i.e. so called “Q-LV” interval). As previously
19 described, pacing at the longest delay site was strongly associated with LV reverse
20 remodeling and the alleviation of symptoms. In addition, multivariable analysis shows that
21 longer Q-LV interval of ≥ 95 ms predicts better CRT response (26). However, the anatomy of
22 the CS vein limits the number of Q-LV measurement sites and can contribute to suboptimal
23 LV lead location.

24

25 *Coronary sinus related anatomical constraints*

1 Several lead-related issues complicate conventional CRT, such as the absence of
2 appropriate CS vein, a challenging CS venous anatomy, lead displacement and high pacing
3 threshold in an area of scar (27). Due to these difficulties, up to 30% of transvenous LV lead
4 placements fail or result in limited or no clinical response, a challenge which may be
5 overcome with the development of new technology (28). Indeed, new quadripolar LV leads,
6 which enable a greater number of pacing configurations, have recently been introduced and
7 were associated with a very low rate of phrenic nerve stimulation and an overall improvement
8 in therapeutic performance (29). Recently, multipoint pacing (MPP) has been developed using
9 a unique quadripolar LV lead and a dedicated algorithm enabling two LV stimulations from
10 two separate dipoles located in the same CS branch (**Figure 1, Panel A**). In early testing,
11 MPP led to more homogeneous electromechanical activation and had significantly better
12 acute hemodynamic response (AHR), functional improvement and reverse remodeling than
13 was achieved through conventional biventricular pacing (30). Currently, the MORE-CRT
14 MPP (MOre REsponse on Cardiac Resynchronization Therapy With MultiPoint Pacing) trial
15 is evaluating the impact of MPP in the treatment of non-responder patients to standard CRT
16 <NCT02006069>.

17

18 Multisite pacing has also been proposed as another LV stimulation configuration
19 (**Figure 1, Panel B**). Indeed, this stimulation scheme uses two leads implanted in two separate
20 CS tributaries aiming to obtain a more rapid and homogeneous LV activation pattern. The
21 approach has been evaluated in a randomized study and appears to be feasible (31) but is
22 associated with a high rate of adverse events and to this point has not shown significant long-
23 term clinical benefits (32).

24

1 **ALTERNATIVE LEAD PLACEMENT FOR LEFT VENTRICULAR STIMULATION**
2 **IN CASE OF FAILED CORONARY SINUS APPROACH**

3

4 Despite the development of multipolar LV electrodes and multipoint pacing, clinical
5 non response due to suboptimal lead positioning remains a critically relevant problem.
6 Additionally, unsuitable CS vein anatomy leads to failed procedures, causing physicians have
7 to propose alternative solutions. Surgical LV epicardial lead, LVendo lead placement or more
8 recently His bundle pacing (HBP) have been described as options to overcome the
9 challenging CS approach.

10

11 *Surgical left ventricular epicardial stimulation*

12 Epicardial LV lead placement through a small lateral thoracotomy or using
13 thoroscopic techniques has been evaluated to overcome these obstacles and has been shown
14 to be feasible (11) (**Figure 1, Panel C**). Furthermore, surgical epicardial LV lead placement
15 can provide the flexibility for lead placement at a position anticipated to have maximal
16 dyssynchrony. However, such an approach is appropriate only if a cardiac surgical service is
17 available in the implanting center. Additionally, previous study showed that epicardial LV
18 lead placement did not result in significant improvement of LVEF or cardiac perfusion (33).
19 Lastly, access to the basal posterolateral aspect of the LV with a surgical lead can be
20 relatively difficult and may not always be achieved in clinical practice (34). Currently,
21 epicardial LV lead indication is mainly limited to re-implantation after device infection or for
22 children with congenital heart disease who need to be permanently paced (35).

23

24 *Endocardial left ventricular stimulation*

1 In some cases of unsuccessful transvenous implantation or non-response to CRT,
2 operators have developed an alternative technique and implanted the LV lead in the LV
3 endocardium through a transseptal atrial or ventricular approach (12) (**Figure 1, Panel D**).
4 The placement of a transseptal LVendo lead was first described in 1998 and has undergone
5 multiple modifications with a superior, inferior, or mixed approach (14). Though this
6 technique is familiar to electrophysiologists, atrial transseptal puncture performed through a
7 superior venous access (subclavian/axillary vein) remains challenging and peri-procedure
8 transoesophageal echocardiography is often necessary to guide operators. Currently, atrial
9 septum is punctured with a needle and ventricular septum puncture is performed using
10 radiofrequency energy (12; 36). Then a balloon/dilatator may be used to dilate the orifice. A
11 wire is placed in the left cavity (atria or ventricular), serving as a guide for the introduction of
12 the stimulation lead through a deflectable sheath. Although complex, the reported procedural
13 success rates are high. The ALSYNC (ALternate Site Cardiac ResYNChronization) study
14 reported an atrial transseptal success rate of 89.4% among the 138 patients treated (37). The
15 steps of the atrial transseptal approach are illustrated in the **Figure 2**. In addition, Gamble *et*
16 *al* described a successful ventricular transseptal approach performed in all the 20 patients
17 recruited with mean time from venous access to passage of the sheath into the LV of 25
18 minutes (12).

19
20 Despite more complex implant procedure, LVendo pacing may bring several
21 advantages compared to the CS approach: 1) operators theoretically have access to all regions
22 of the LV, 2) potentially faster LV depolarization resulting from faster impulse propagation in
23 the endocardial ventricular layers than the epicardial ones, 3) more physiologic LV
24 stimulation, preserving the transmural activation and repolarization sequence, and 4)
25 elimination of phrenic nerve stimulation as a concern (14;15). Indeed, Derval *et al.* tested

1 endocardial and epicardial pacing at the exact same location in human subjects and showed
2 that LVendo pacing provided a significant benefit in diastolic, but not systolic function (22).
3 In addition, the study showed that the best sites were frequently accessible only via the
4 endocardial approach. LVendo pacing has also been evaluated in ischemic cardiomyopathy
5 with poor response to conventional CRT (38). In this study, 8 patients underwent cardiac
6 magnetic resonance mapping which was compared to extensive invasive electroanatomic
7 mapping to target optimal LVendo pacing sites and avoid the scar areas. A total of 135
8 epicardial and endocardial sites were evaluated during this study. LVendo pacing showed
9 superior AHR as well as shorter stimulation-QRS duration and paced QRS compared to CS
10 pacing. Of note, in 6 of 8 patients, there was no correlation between the optimal LVendo site
11 and the site of latest electrical activation on electroanatomic mapping due to slow conduction
12 areas inside islands of scar.

13
14 Concretely, the efficacy of LVendo lead has been evaluated in the ALSYNC study that
15 enrolled a population who had previously failed to conventional CRT implantation or
16 classified as non-responder to CRT (37). The study showed that 55% and 59% of patients had
17 a reduction in LV end-systolic volume of at least 15%, and achieved an improvement by ≥ 1
18 NYHA class, respectively. Of note, 33% of the patients showed ‘super-response’ at 6 months.
19 Recently, a meta-analysis estimated the clinical response rate as 82% using this approach
20 (39).

21
22 Despite these advantages, there are some drawbacks of this strategy. The main and
23 most serious concern is the risk of thrombo-embolic events that requires long-term
24 anticoagulation. In the ALYNCS study, 6-month after implantation, 17.8% patients had at
25 least one endocardial LV lead-related complication, with an incidence of thrombo-embolic

1 and transient ischemic attack events at 2.6 and 7.4 per 100 patient-years; respectively (37).
2 Similar results were found in a meta-analysis with an incidence of stroke and transient
3 ischemic attack of 2.5 and 2.6 events per 100 patient-years (39). In addition, this procedure
4 necessitates a transseptal puncture to reach the LV, which holds inherent risks.

5

6 In the light of these results and associated complications, endocardial pacing shows
7 promise with a more physiological LV stimulation compare to CS pacing. However, the
8 endocardial lead remains a critical shortcoming of this approach, given the associated risk of
9 stroke, the need for long-term of vitamin K antagonist therapy and drug monitoring. In
10 addition, atrial or ventricular transseptal approaches add difficulty to the CRT implantation
11 procedure (12).

12

13 *Resynchronization using His bundle pacing*

14 Permanent HBP has recently emerged as a more physiological form of ventricular
15 pacing and viable alternative to CRT. Indeed, previous study demonstrated that His
16 resynchronization is achieved by recruiting LV conduction fibers (40). Briefly, the dedicated
17 *SelectSecure* HB pacing lead (Medtronic Inc, Minneapolis, MN) is delivered through a fixed
18 curve sheath or a deflectable sheath. During procedure, HB electrograms are carefully
19 mapped and paced with the dedicated lead until pacing recruited the diseased bundle and
20 narrowed the QRS duration by at least 20%. The lead is then screwed into position by means
21 of 4–5 clockwise rotations. Of note, the HB is surrounded by fibrous tissue and the average
22 capture thresholds tend to be higher than routine RV pacing but capture thresholds above
23 2.5V/1ms would must make the operator consider re-implantation lead (41).

24

1 Feasibility and safety of HBP CRT eligible patients have been demonstrated among
2 106 CRT candidates or patients with failed conventional approach. In this cohort, HBP was
3 successful in 90% and both groups experienced significant QRS duration narrowing (from
4 $157\pm 33\text{ms}$ to $117\pm 18\text{ms}$). Additionally, HBP patients exhibited clinical and
5 echocardiographic improvement during follow-up but with 7% of loss of bundle branch
6 recruitment (42). Similarly, hemodynamic performance and electrical activation mapping
7 have been compared using HBP and conventional biventricular pacing (43). Authors
8 demonstrated that acute hemodynamic response was higher when delivered using HBP than
9 bi-ventricular pacing. Furthermore, activation map obtained during HBP showed resolution of
10 the LBBB and provided more homogeneous LV resynchronization than bi-ventricular pacing.
11 Lastly, current study highlighted the promising results of CRT using HBP in patients with
12 right BBB and reduced LVEF (44). Currently, the HIS-SYNC (His Bundle Pacing versus
13 Coronary Sinus Pacing for Cardiac Synchronization Therapy) trial is comparing HBP to bi-
14 ventricular pacing and should provide important information regarding the impact of
15 resynchronization using HBP <NCT02700425>.

16

17 In the light of these data, HBP seems hopeful for CRT and when compared to LVendo
18 lead, this techniques avoids the thrombo-embolic and transseptal puncture risks. However, the
19 biggest limitation of permanent HBP is the inability to map the HB and perform implantation
20 of the lead at the HB in 10% of cases. Additionally, the need for higher pacing output might
21 result in shorter battery longevity of devices. Lastly, endocardial lead remains the Achilles
22 heel of HBP.

23

24 **LEADLESS LEFT VENTRICULAR PACING: THE NEXT ADVANCE FOR**
25 **PATIENTS WITH A FAILED CORONARY SINUS APPROACH?**

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Evidence of left ventricular leadless pacing benefit

Despite significant advances, transvenous leads have remained the greatest weakness of pacing devices. In an attempt to address these lead-related acute and chronic complications, leadless cardiac pacing has been developed. The last technological prowess is probably the development of CRT using a leadless endocardial LV electrode (**Figure1, Panel E**) (WiSE-CRT, EBR Systems, Sunnyvale, California). Recently, a case of an entirely leadless CRT was published, providing a tantalizing view of the potential future of CRT (45) (**Figure 1, Panel F**).

Briefly, the WiSE-CRT system provides wireless pacing by transmitting acoustic energy from a pulse generator transmitter, implanted subcutaneously above an intercostal space, to a receiver electrode implanted in the LV wall, which converts the acoustic energy to electrical pacing energy. The WiSE-CRT System is co-implanted with any pacemaker, ICD, or CRT device, which provides RV pacing. Biventricular pacing is achieved by sensing the RV pacing signal of the co-implant device, and using it as a trigger for LV stimulation. Implanting the WiSE-CRT System typically requires a 2-step process. First, the pulse generator system is surgically implanted in one of the left subcutaneous intercostal spaces (4th to 6th) adjacent to the parasternal border. Second, the wireless electrode is implanted in the LV wall with anchor barbs via a transaortic retrograde or transseptal approach. In addition to the leadless pacing advantages, LV electrode could offer the opportunity for congenital heart disease and a uni-ventricular heart to receive minimally invasive non thoracotomy pacing systems.

The feasibility and safety of the WiSE system was evaluated in the WiSE-CRT (Wireless Stimulation Endocardially for CRT) study (46). Seventeen patients were enrolled

1 and at 6-month follow-up, all the implanted patients (n=13) were alive, though 7 serious
2 adverse events occurred in 6 patients (35%). The system performance was also assessed with
3 biventricular pacing recorded in 92% of the patients at 6 months. In addition, two-thirds of the
4 patients had at least one functional class change and a significant 6-point increase in LVEF.
5 However, because of a very high incidence of pericardial tamponade (18%), the study was
6 stopped after 17 patients. A new generation device was developed with the addition of a
7 balloon to facilitate atraumatic engagement with the LV endocardium. Recently, the
8 SELECT-LV study evaluated the performance of the new version of the wireless electrode
9 (47). A total of 39 patients were enrolled and 35 underwent the procedure, which was
10 successful in 34 patients. Of note no pericardial effusions occurred. At 6-month follow-up, bi-
11 ventricular pacing was achieved in 93.9% of patients and 84.8% had improvement in the
12 clinical composite score. During follow-up, one pocket hematoma and two confirmed
13 subcutaneous device-related infections occurred and device extraction was performed in one
14 patient. Future planned enhancements, such as a smaller pulse generator and different delivery
15 catheter designs are in development, which may reduce the risk of complications. Currently,
16 the SOLVE-CRT (Stimulation Of the Left Ventricular Endocardium for Cardiac
17 Resynchronization Therapy in Non-Responders and Previously Untreatable Patients) study
18 was recently launched to evaluate the safety and efficacy in a cohort of 350 patients and will
19 probably provide stronger benefit information < NCT02922036>.

20

21 *How to achieve the optimal LV electrode placement site*

22 The optimal LVendo pacing location exhibits marked variability in ischemic and non-
23 ischemic cardiomyopathy and physicians may use a combination of either preprocedural or
24 periprocedural imaging and/or electrophysiology mapping criteria to identify the best pacing
25 sites. Recently, a multicenter study hypothesized that guided the placement of the wireless

1 pacing electrode would achieve greater improvements in CRT response (48). Different
2 strategies were used: 1) echocardiography to identify the latest mechanical activated LV
3 segment, 2) cardiac magnetic resonance determined the latest activation area and scar, 3)
4 electro-anatomical mapping to identify areas with late electrical activation and low voltages
5 or 4) electrical latency parameters (i.e. Q-LV duration and Q-LV/QRS ratio) (49). In the 4th
6 approach, Q-LV interval <100ms were excluded and the viability was assessed by excluding
7 any sites with a pacing capture threshold >2V. During each procedure, AHR was measured to
8 assess the immediate response to LVendo pacing. The target site identified with pre-
9 procedural imaging was reached in 92% of patients and a strong linear relationship between
10 AHR and both Q-LV and Q-LV/QRS ratio was observed, especially in the case where the Q-
11 LV/QRS ratio was >0.5 at the pacing site. This suggests that patients will be more prone to a
12 reverse remodeling if a site with a LV/QRS ratio of >0.5 is selected. Results showed that
13 guidance for the optimal site selection of a wireless LV electrode improves chronic reverse
14 remodeling at a rate of 71% and thus may increase the rate of responders to CRT. **Figure 3**
15 synthesizes the main strategies used to guide LVendo lead implantation and proposes concrete
16 clinical application.

17

18 *Limits of the wireless left ventricular electrode*

19 There are several potential limitations to the wireless LV electrode approach. First, for
20 optimal LVendo pacing, the transmitter must target the electrode to efficiently focus acoustic
21 energy. A severe angulation or a large distance (>10cm) between the transmitter and electrode
22 reduces the system efficiency. To address this, the location, distance, and angle of the
23 electrode are tracked in real time during implantation by the transmitter's tracking algorithm.
24 Moreover, the system requires an acoustic window in order to transmit ultra-sound
25 effectively. Second, in case of large dilated cardiomyopathy, it may be difficult to reach some

1 areas of left lateral free wall, since the current delivery sheath has one unique curve, which
2 could limit implantation in the basal area. Lastly, similarly to LVendo lead complication,
3 thromboembolic events could occur in patients implanted with a WiSE electrode.

4 5 *Future direction*

6 Recently, two novel resynchronization techniques seem promising: HBP and LV
7 wireless electrode. However, trans-venous lead implantation are still required for both
8 techniques (HB stimulation for the first one and RV pacing detection for the second one). The
9 future of the CRT might be written in the combination of these two systems and the
10 development of leadless HBP leading to an entirely leadless resynchronization using a mono-
11 electrode.

12 13 **CONCLUSION**

14
15 Several methods have been proposed to improve CRT and decrease unsuccessful
16 procedures, each with advantages and disadvantages (**Figure 4**). While current alternatives to
17 optimize LV stimulation using surgical epicardial leads or LV endocardial leads have shown
18 promise, none have proved to be ideal. Recently, HBP has demonstrated interesting results
19 and represents promising alternative to conventional bi-ventricular pacing. Lastly, leadless
20 endocardial strategy provides an individualized optimized LV lead location coupled with
21 more physiological endocardial activation. Future clinical use and randomized clinical trials
22 will help us to evaluate the safety and efficacy of this invasive technique and clarify the place
23 of LV leadless stimulation in our current clinical practice.

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- 3

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6
7

1 **FIGURE TITLES AND LEGENDS**

2

3 **FIGURE 1:Evolution of the LV pacing sites.** Panel A=Multipoint pacing, Panel
4 B=Multisite pacing with two LV lead in the CS (triangles), Panel C=Surgical epicardial lead
5 (square), Panel D=LV endocardial lead using an atrial transseptal approach (arrow), Panel
6 E=LV endocardial leadless with the WiSE electrode (star), Panel F=Entirely leadless CRT
7 with a Micra pacemaker (arrow) and WiSE electrode (star).

8 CRT=Cardiac resynchronization therapy; LV=Left ventricular

9

10 **FIGURE 2:Illustration of atrial transseptal approach.** Panels 1 to 4 represent the different
11 steps from transseptal puncture to LV lead placement. Adapted from Morgan *et al* (38).
12 Reproduced with permission from the European Heart Journal.

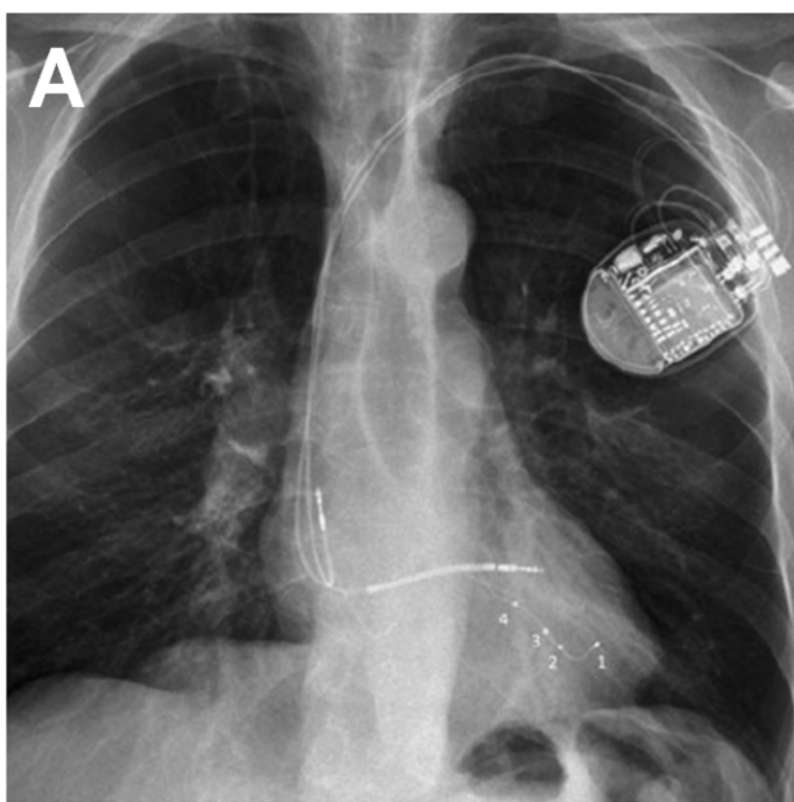
13

14 **FIGURE 3:Main strategies described to guide LV electrode implantation and suggested**
15 **clinical practice application.** CMR=Cardiac magnetic resonance; LV=Left ventricular.

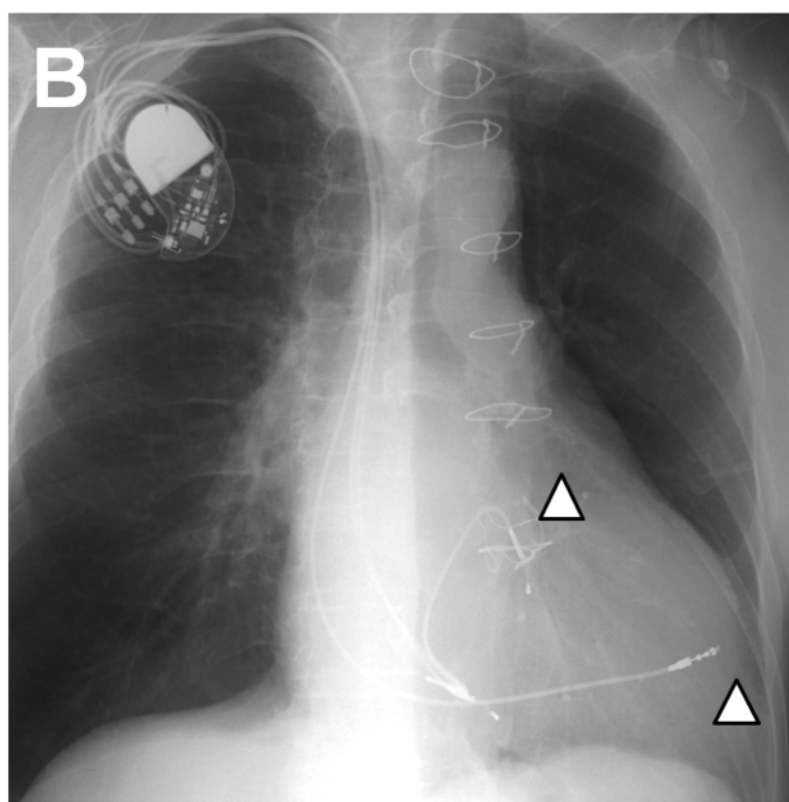
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17 **FIGURE 4:Advantages/disadvantages of current approaches, alternative and future**
18 **directions for LV pacing.** LV=Left ventricular.

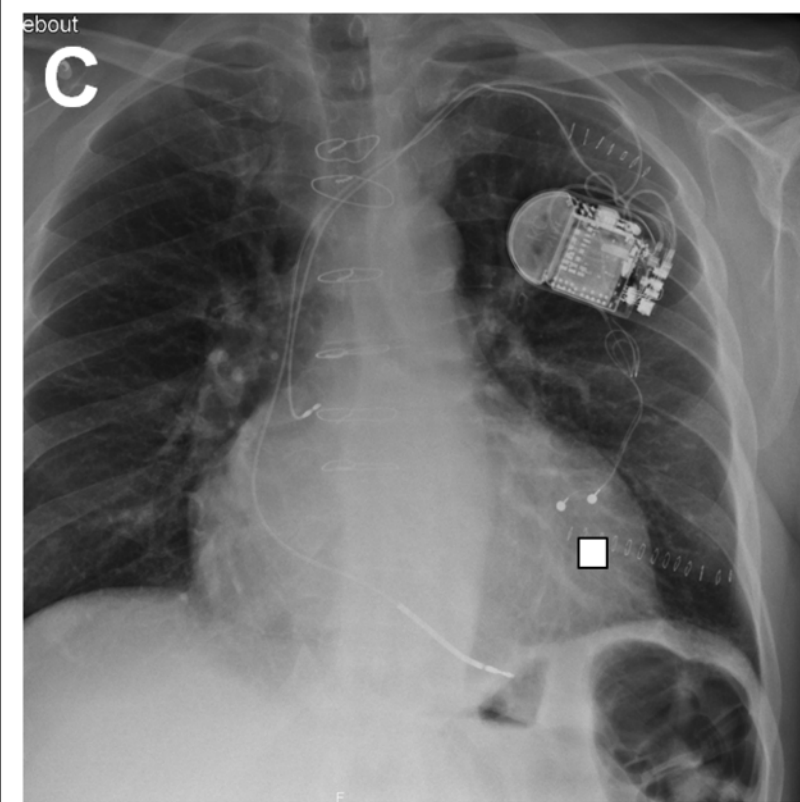
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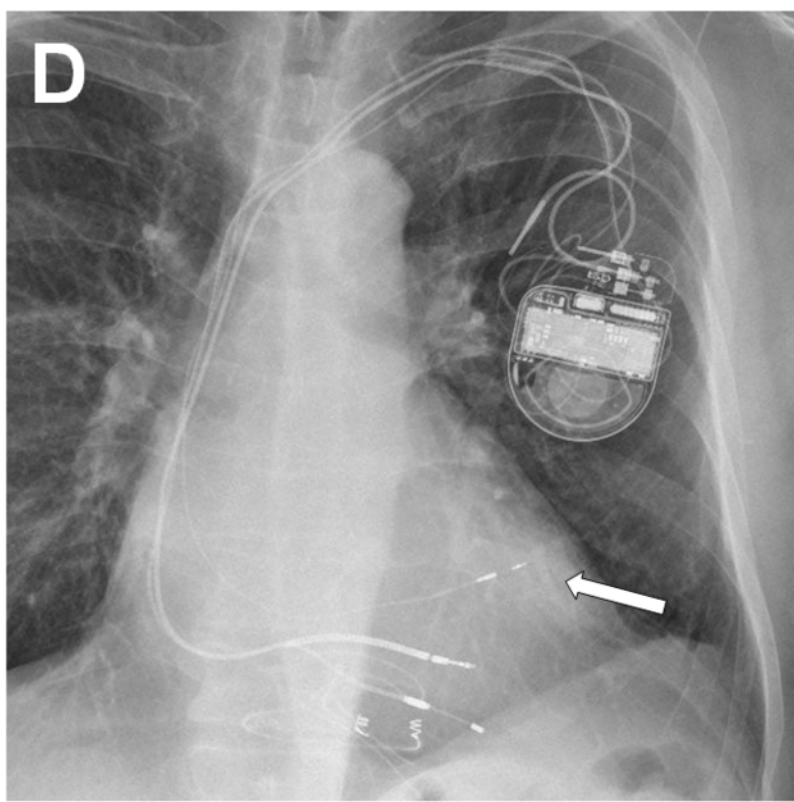
Multipoint pacing



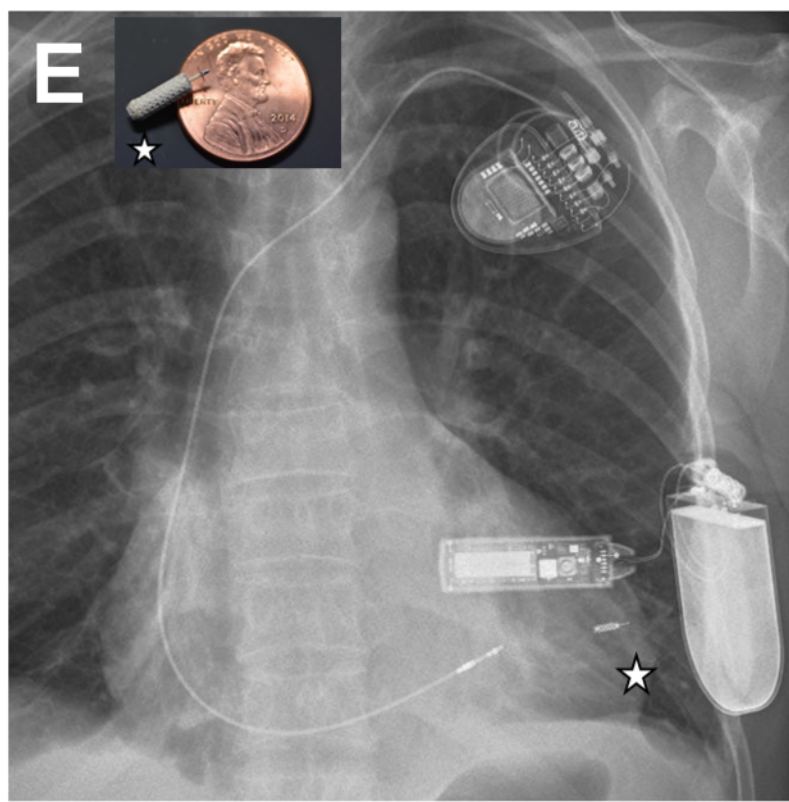
Multisite pacing



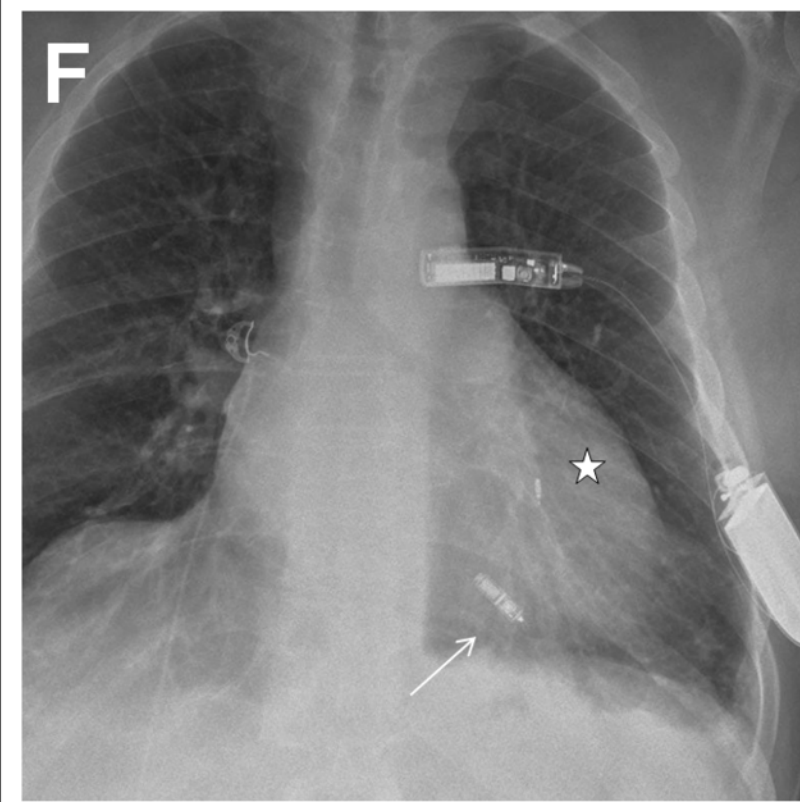
Surgical epicardial LV lead



Transseptal endocardial LV lead



WiSE electrode



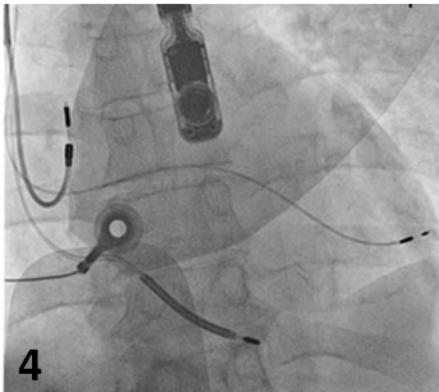
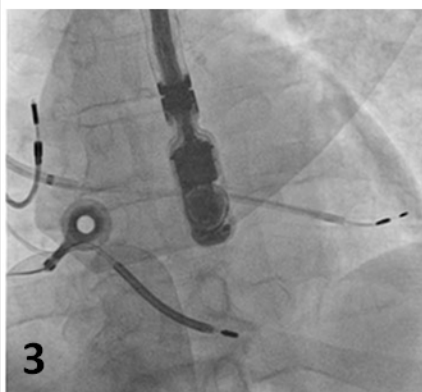
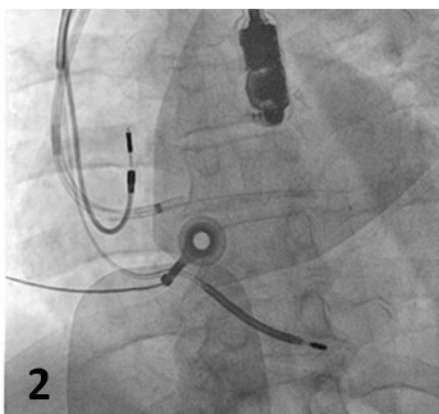
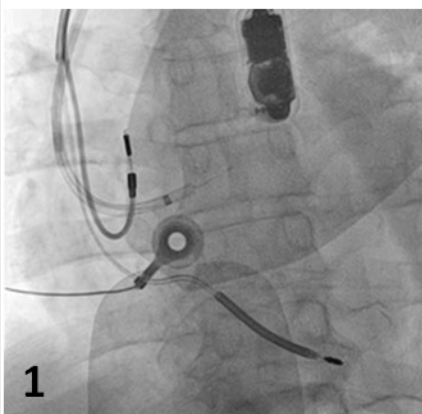
Entirely leadless CRT

ETO
X7-2t
44Hz
11cm

T. P.M.: 37,0 °C
T. ETO: 30,6 °C
0 56 100

2D
Gén
Gn 70
C 50
4/2/0
75 mm/s

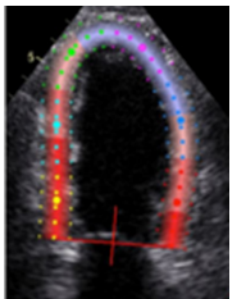
G
P R
3,0 0,0



PRE PROCEDURAL

GUIDANCE STRATEGIES

Echocardiography
Speckle tracking

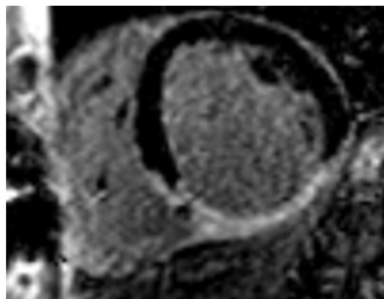


Identify the latest
mechanical activated
LV segment

Target pacing site



CMR



Identify LV scar areas

Site to avoid

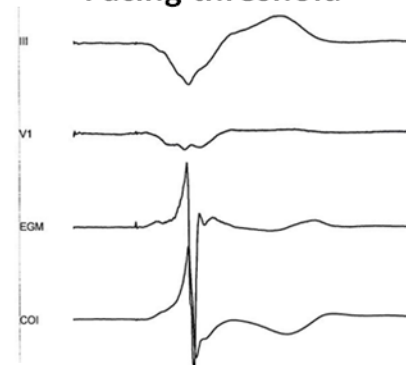


OBJECTIVES

PERI PROCEDURAL

Electrical parameters

Q-LV interval
Q-LV/QRS ratio
Pacing threshold



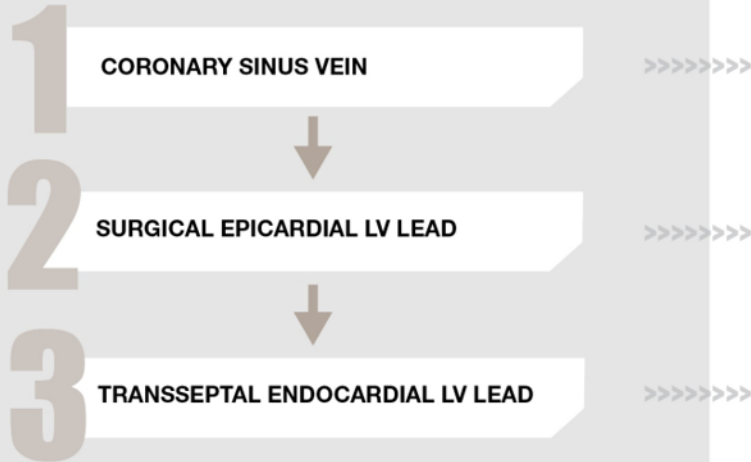
Q-LV interval > 100ms
Q-LV/QRS ratio > 0.5
Pacing threshold < 2V

Position the WiSE electrode



CURRENT CLINICAL ALGORITHM FOR ALTERNATIVE APPROACH IN CRT AND FUTUR DIRECTION

CURRENT STRATEGY



ADVANTAGES

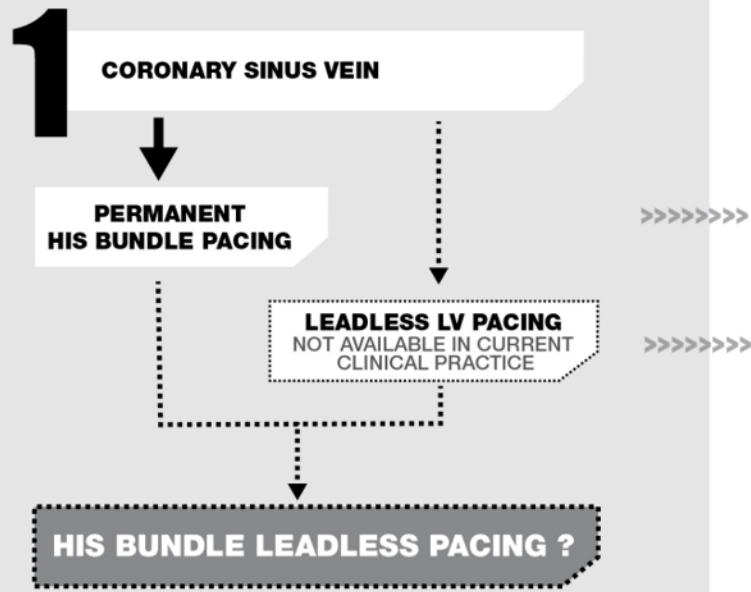
- Conventional approach with high level of evidence
- Well managed technique
- New technology improvement
- Higher flexibility for LV lead location
- Endocardial pacing (more physiological LV simulation)
- Access to all LV regions
- No phrenic nerve pacing



DISADVANTAGES

- Electrical constraints
- High threshold pacing
- Limited location possibility
- Phrenic nerve stimulation
- Need for a surgical team
- Increased procedural risk
- Posterolateral LV wall can be difficult to target
- Need for a transeptal puncture
- Ischemic stroke risk
- Long-term anticoagulation

NEW STRATEGY AND FUTUR DIRECTION



- Physiological stimulation
- Shorter QRS narrower and better LV activation than biventricular pacing
- Currently available on market
- No transvenous lead
- Endocardial pacing
- No anticoagulation

- Transvenous lead
- High pacing threshold
- Technical procedure
- Recent technology with few hinsight
- Need for an acoustic window
- Complex procedure with various implantation parameters to achieve